

1 **TITLE**

2 DNA delivery to “ex vivo” human liver segments

3

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27 **Running title:** Naked DNA delivery to *ex vivo* human liver segments

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33 ABSTRACT

34 Hydrodynamic injection is an efficient procedure for liver gene therapy in rodents but
35 with limited efficacy in large animals, using an “in vivo” adapted regional
36 hydrodynamic gene delivery system. We study the ability of this procedure to mediate
37 gene delivery in human liver segments obtained by surgical resection. Watertight liver
38 segments were retrogradely injected from hepatic vein with a saline solution containing
39 a plasmid bearing the eGFP gene, under different conditions of flow rate (1, 10 and 20
40 ml/s) and final perfused volume. Samples were cultured 1-2 days and used for
41 microscopy and molecular analysis of gene expression. The fluorescent and
42 immunohistochemistry studies indicated that in segments injected at ≥ 10 ml/s, good and
43 wide gene expression is present in the liver sections and the molecular analysis
44 reinforced the histological observation in a quantitative manner (index of apparent gene
45 delivery: 10^2 - 10^4 eGFP DNA copy/100 pg of total DNA; transcription index: 10^5 - 2×10^6
46 eGFP RNA copy/100 ng of total RNA). In addition, injected gold nanoparticles (15 nm
47 diameter) suggested that DNA delivery to hepatocytes must involve a facilitated
48 permeation process without membrane disruption. In summary, we show that retrograde
49 venous injection of watertight human liver segment is an anadromous procedure that
50 results in wide liver gene delivery and good gene expression. However, additional
51 studies will be necessary to clarify the influence of the prolonged ischemia injury to
52 hepatocytes in our model.

53

54 **Key words:** Gene delivery, human, liver, catheter, naked DNA, hydrodynamic

55 INTRODUCTION

56 The present study has been designed to explore the capacity of regionally hydrodynamic
57 gene delivery to human liver segments, employing an “ex vivo” catheterization
58 procedure. Hydrodynamic gene transfer^{1,2} with naked DNA is a safe and efficient
59 method for gene delivery, and we had reported advances in the efficacy of naked DNA
60 gene delivery to mice liver, resulting in long-term therapeutic plasma levels of the
61 protein encoded by the exogenous gene². Since the suggested mechanism underlying the
62 important efficacy of liver gene delivery involves transient inversion of intraorgan
63 blood flow, we had the opportunity to improve the technique and apply it to larger
64 animals, using catheterization procedures – as suggested by preliminary results from
65 both other authors and our own group³⁻⁵. The gene expression efficiency achieved by
66 this procedure is lower than that achieved by the original mouse procedure involving
67 hydrodynamic tail vein injection². However, the results suggest that liver gene therapy
68 is a promising strategy in which the large liver size and/or the less compliant connective
69 tissue framework of large animals limit the efficiency of liver gene transfer. In this
70 respect there is experimental evidence that promising results are achieved in less elastic
71 cardiac tissue⁶, and that outflow obstruction during DNA hepatic vein injection
72 significantly contributes to increase the efficiency of hydrodynamic liver gene delivery⁷.
73 Since all blood vessels are sealed in surgically derived human liver segments, we
74 employ such watertight liver segments to evaluate the efficacy of anadromous naked
75 DNA delivery mediated by hydrodynamic retrovenous injection.

76 The present study shows that catheter-mediated retrograde injection of naked DNA
77 bearing the eGFP marker gene in the hepatic vein of “ex vivo” human liver segments
78 results in wide anadromous gene delivery and gene expression, without dramatic
79 morphological changes in the liver tissue as evidenced by electron microscopy and the
80 liver distribution of 15 nm gold particles. We must take into consideration that having
81 performed our experiments in liver ischaemic segments of patients undergoing resection
82 due to hepatic cancer, additional experiments are required to confirm the results in a less
83 prolonged ischaemic situation.

84

85 RESULTS

86 *Catheterization*

87 The catheter was placed in hepatic vein of the liver segment, and vascular permeation of
88 the liver segment was monitored by fluoroscopy after the injection of contrast solution.

Figure 1 is representative of all the experiments and shows the fluoroscopic position of the catheter with respect to its anatomical location (A and B panels) and the vascular tree after the injection of 5 and 10 ml of contrast solution (C and D panels), respectively. The place where liver samples were taken for molecular analysis can be observed in panel B, corresponding to the right direction of injection, zone A samples, and lateral perfusion areas, zone B samples. We cannot know if contrast solution injection affects eGFP expression since we have injected contrast in all our experiments. For this reason, we always have tried to employ the minimum necessary quantity (volume $\leq 1\%$ segment weight).

Histological study of eGFP expression

Three different groups were analyzed by fluorescence and/or immunohistochemical procedures. One was injected at 20 ml/s, 1/10 volume of segment weight and gene expression was evaluated by fluorescence microscopy (Fig. 2: A, B, C). The second group was injected at 10 ml/s, 1/5 volume of segment weight and gene expression was evaluated by immunohistochemistry (Fig. 2: E, F, G). The last group was injected at 1 ml/s, 1/5 volume of segment weight and gene expression was evaluated by both fluorescence (Fig. 2D) and immunohistochemistry (Fig. 2H) procedures. Then, small liver samples (1x0.5 cm) measuring < 1 mm in thickness were cultured, and one and two days after gene transfer we studied eGFP gene expression in histological liver sections, employing fluorescent and immunohistochemical procedures. The results show that one day after injection, the fluorescence was clearly observed and widely distributed in liver cryosections from liver segments injected at a 20 ml/s and 1/10 of the segment weight (Fig.2: A-C), thus suggesting that efficient gene delivery was achieved by this procedure. Immunohistochemistry was also employed to detect eGFP expression. In these experiments, injection was performed at 10 ml/s flow rate and with 1/5 segment weight volume. Specific immunostaining one day after injection in paraffin sections from formalin fixed liver samples is observed in Figs. 2F and G, as compared to immunohistochemistry control performed in absence of specific primary antibody (Fig. 2E). In contrast, in livers injected with 1ml/s, volume of 1/5 segment weight, a very limited fluorescence was observed in two of the four liver segments studied. Even in those cases, only two or three microscopic fields of the whole histological section showed a very light fluorescence (Fig. 2D). Moreover, in our hands, the immunohistochemistry staining was negative in all cases (Fig. 2H).

123 Although the expected reactivity must be lower than with cryosections from frozen
124 samples, a positive reaction was clearly observed in groups injected at 10 ml/s speed or
125 more; however, comparative efficacy determination between the two procedures
126 required molecular analysis.

127

128 *Quantitative PCR and RT-PCR assays of eGFP*

129 In order to determine the influence of flow rate (20 vs 10 ml/s vs 1 ml/s) and total
130 volume (1/10 vs 1/5 segment weight) of the injection upon gene transfer efficacy, we
131 included an additional group (flow rate 20 ml/s and 1/5 ml volume of segment weight)
132 in the above described histochemical study resulting in the following groups: 20 ml/s
133 (1/10 vol), 20 ml/s (1/5 vol), 10 ml/s (1/5 vol), 1 ml/s (1/5 vol) whose pressures during
134 hydrodynamic injection, in the tip of the introducer, were 122.0 ± 102.1 , 190.8 ± 79.4 ,
135 93.4 ± 33.4 and 25.0 ± 12.3 mm Hg, respectively.

136 After liver segment transfection, performed as explained in Methods, cultured samples
137 were collected on days 1 and 2 after transfection to evaluate the index of both apparent
138 gene delivery and transcription, on the basis of the number of molecule copies,
139 employing quantitative PCR and RT-PCR, respectively. Several samples were collected
140 from each segment after injection, always belonging to tissue areas corresponding to
141 those seen to be perfused by the contrast pre-injection. The gene expression data
142 obtained were not significantly different between samples A and B from each segment,
143 being A the area directly perfused and B the areas corresponding to lateral zones. The
144 index of apparent eGFP gene delivery to liver tissue was evaluated as the ratio of eGFP
145 DNA copies per 100 pg of total DNA. The term “apparent” tries to remark that the
146 index evaluates the total amount of DNA present in the tissue, without differentiating
147 the functional ability. The results are summarized in Figure 3A, and indicate that the
148 transgene was present in all liver tissue samples but significant differences were
149 observed between groups: maximal values were observed in the 20 ml/s, 1/5 group,
150 being statistically different from all other groups in zone A at the second day ($p < 0.01$).
151 The transcription index was evaluated as the amount of eGFP RNA copies per 100 pg of
152 total RNA. The results are summarized in Figure 3B, and indicate that the transgene
153 was present in all liver tissue samples from segments injected at ≥ 10 ml/s reaching
154 from 10^5 to 2×10^6 copies per 100 ng total RNA, approximately. In all cases, the highest
155 values were observed on day 2 after transfection, but no statistically significant

156 differences were observed between groups. However, once again, lower values were
 157 observed in segments injected with 1 ml/s, 1/5vol ($p < 0,05$, zone B, day 2).
 158 The apparent intrinsic gene efficacy (iE) indicates the amount of RNA produced per
 159 gene copy, and was evaluated as the ratio of RNA/DNA copy of eGFP in each sample.
 160 We must note that this parameter, as its name indicates, is “apparent”, so the values
 161 must be interpreted in the context of the experiment, so the presence of extracellular or
 162 non functional plasmids cannot be excluded, but it should be an interesting parameter
 163 for the relative comparison between groups. The results are summarized in Figure 4,
 164 and show that higher apparent iE, 10^4 approximately, was observed in the liver
 165 segments transfected with the injection flow rate of 10 ml/s, 1/5 vol, and continued to
 166 show similar values on days 1 and 2 post-transfection, being significantly different (p
 167 $< 0,01$) to all the other groups. However, in the segments transfected with 20 ml/s,
 168 apparent iE was lower (10^3) and decreased one order of magnitude in samples from
 169 zone A, day 2 with respect to day 1, mainly when the highest final volume (1/5 of
 170 segment weight) was employed. Since iE is largely dependent on cell viability, we
 171 suspect that mild transfection conditions should offer cellular advantages for gene
 172 expression, as higher flow and volume values could mediate cell damage resulting in a
 173 time-dependent gene iE decrease. When perfusion conditions are too slow (1ml/s), the
 174 intrinsic efficacy is dramatically reduced (10^{-1} approx.), suggesting that the functionality
 175 of the delivered DNA must be very limited. Regarding A and B zones, significant
 176 differences between them were only found in 10 ml/s, 1/5 group ($p < 0,01$).
 177
 178

179 *Transmission electron microscopy*

180 Relevant morphological changes in the liver after hydrodynamic injection, mainly
 181 endothelial disruption and massive endocytic vesicles in hepatocytes, have been
 182 previously described in mouse and pig^{2,4,5,8}. To confirm whether these morphological
 183 changes also occur in humans, the liver segments were retrogradely injected at a 20 ml/s
 184 flow rate with buffered 2.5% glutaraldehyde solution. Then, tissue samples were
 185 collected for transmission electron microscopy. Figure 5 shows a representative image
 186 at low magnification of a venous sinusoid and four details (boxes a, b, c and d), at
 187 higher magnification, of different areas containing vascular endothelium, Disse space
 188 and apical hepatocytes. The main morphological changes observed were: a) dilated
 189 sinusoid; b) very small changes, if any, in the sinusoidal endothelium, without signs of

190 disruption; and c) dilated space of Disse at some sites, without massive endocytic
191 vesicles in the hepatocytes. The morphological changes observed in the liver were
192 smaller than expected, suggesting that anadromous DNA delivery to hepatocytes must
193 involve facilitated permeation, not a membrane disruption process.

194 In order to reveal the possible existence of membrane disruption not directly observed
195 by transmission electron microscopy, other liver segments were retrogradely injected at
196 a 20 ml/s flow rate with buffered 2.5% glutaraldehyde solution containing gold
197 nanoparticles (15 nm in diameter and 10^{12} particles/ml). Because large amounts of gold
198 nanoparticles are necessary for these experiments, the particles were prepared as
199 described in Methods. The morphological characteristics of the nanoparticles and the
200 diameter distribution are presented in Figure 6. The mean nanoparticle diameter
201 employed in this experiment was 15.5 ± 0.3 nm. The gold nanoparticle distribution in
202 the liver segment is shown in Figure 7, where the central image (at low magnification)
203 shows a dilated sinusoid in which specific boxes, corresponding to sites of the
204 endothelium-Disse space-hepatocyte (a, b, c, d), are amplified with the aim of
205 identifying the location of nanoparticles. In all cases, nanoparticles were observed
206 inside the sinusoid or within the Disse space. In no case were nanoparticles observed
207 inside the hepatocytes, thus suggesting the absence of any hepatocyte membrane
208 disruption, and the implication of a facilitated permeation process in DNA delivery to
209 the liver cells.

210

211 DISCUSSION

212 The present work shows that anadromous gene delivery to “ex vivo” human liver
213 segments, mediated by retrograde injection of naked DNA encoding for the eGFP gene
214 in the hepatic vein, results in efficient gene transfer as indicated by: a) eGFP DNA,
215 RNA identified by quantitative PCR, RT-PCR, and b) eGFP protein identified by
216 fluorescent and immunohistochemistry procedures. In our hands, the best of the studied
217 conditions for transfection was retrograde injection of a saline solution of eGFP plasmid
218 (20 μ g/ml) at a flow rate of 10 ml/s and a final volume equivalent to 1/5 of the liver
219 segment weight in grams; and c) the ultrastructural studies employing gold
220 nanoparticles suggest that the mechanism of gene delivery must be mediated by a
221 facilitated permeation process, not by hepatocyte membrane disruption.

222 Important progress has been made in nonviral gene therapy since the hydrodynamic
223 procedure for mouse liver gene delivery was first described^{2,8-10}. However, the systemic

224 perturbation resulting from hydrodynamic injection remains a serious limitation for
 225 clinical application, since it can lead to circulatory collapse and even death. To avoid
 226 this adverse effect, we have described a retrograde catheter-mediated gene delivery
 227 procedure⁵ with the aim of locally reproducing the intrahepatic conditions mediated by
 228 tail vein hydrodynamic injection. However, all the studies reported in pigs^{4,5,11-14} and in
 229 human clinical trials³ indicate that the efficiency of the procedure remains several orders
 230 of magnitude lower than observed in mice. The exact reason for the low gene transfer
 231 efficiency of retrograde injection is still unknown, but the low resistance of the sinusoid
 232 bed must be a very important factor, since DNA can easily travel across the liver
 233 segment after hepatic vein injection, reaching the portal vein and then freely returning to
 234 the inferior cava vein through another liver segment¹⁵.

235 In the present work, we hypothesize that human “ex vivo” liver segments must be
 236 excellent candidates for anadromous gene transfer, since the outflow of injected DNA
 237 solution from the targeted segment is blocked in the surgical removal process. In all
 238 cases, vascular patency before injection was confirmed by contrast injection and Rx
 239 fluoroscopy. The injection conditions were similar to those employed in pig
 240 experiments for catheter mediated “in vivo” gene transfer, but with the advantage of
 241 blocking outflow of injected DNA solution. The results indicate that both 20 and 10
 242 ml/s injection flow rates of a plasmid saline solution (20 µg/ml) containing the eGFP
 243 gene mediate efficient gene transfer, as observed by light microscopy employing direct
 244 fluorescence or immunohistochemistry procedures. This observation confirms the
 245 preliminary hypothesis and supports the idea that outflow obstruction during DNA
 246 hepatic vein injection significantly contributes to increase the efficiency of
 247 hydrodynamic liver gene delivery⁷. However, when segments were injected with high
 248 volumes (1/5 vol) but low flow (1ml/s) we hardly find the protein expression in
 249 histological sections. The microscopic observations support the good efficacy of gene
 250 delivery in groups injected with ≥ 10 ml/s, but the eGFP gene encodes for a non-secreted
 251 protein that accumulates within the cytoplasm, and therefore the amount of protein is
 252 poorly correlated to expression efficacy.

253 In order to evaluate how delivery and transcription of the eGFP gene contribute to liver
 254 gene transfer efficacy, two tissue indexes were used based on the number of DNA or
 255 RNA copies. The eGFP gene apparent delivery index (DNA copy number per 100 pg of
 256 total DNA) was 10^2 to 10^4 eGFP copies per 100 pg of total DNA, approximately. The
 257 liver segments injected with 1 ml/s also showed lower index values. Interestingly, the

value of the index decreases as the injection conditions become milder (in general, 20
 ml/s $1/5 > 20$ ml/s $1/10 > 10$ ml/s $1/5 > 1$ ml/s $1/5$). However, we must remark that this
 index is of apparent distribution, and so it does not analyze the functionality of the
 quantified DNA. Given that the copy number reached by the milder conditions is 10^2 ,
 we could think that a great part of the injected DNA could reach the tissue but without
 functional ability, as supported by histochemical studies summarized in Fig. 2. If we
 consider that 3,3 pg DNA is equivalent to a haploid human genome¹⁶, our results
 suggest an equivalent efficacy of 10-1000 eGFP gene copies/cell, approximately.
 The eGFP gene transcription index (RNA copy number per 100 ng of total RNA) was
 10^5 to 2×10^6 copies per 100 ng total RNA, approximately, in groups injected with $\geq$
 10 ml/s, but 2-3 orders of magnitude lower when injected with 1 ml/s, 1/5 vol. In all
 cases, the highest values were observed two days after transfection in groups injected at
 ≥ 10 ml/s. Although no significant difference was observed between those groups, the
 liver segments injected with 10 ml/s showed slightly higher index values at day one post
 injection.

The apparent gene intrinsic efficacy (iE) (RNA/DNA copy number of a gene) is an
 interesting parameter, because it indicates gene cell functionality on the base of the
 efficacy of gene delivery and transcription in the tissue sample. We must note that this
 “apparent” parameter must be interpreted in the context of the experiment. The presence
 of extracellular or non functional plasmids cannot be excluded, therefore in those cases
 in which the proportion of extracellular plasmids was very elevated, the indexes could
 not be accurate measures of the efficiency. Anyway, they could be interesting
 parameters for the relative comparison between groups. Our results indicate that
 apparent iE decreased 10 times from day 1 to 2 after transfection in both groups of liver
 segments injected at a 20 ml/s flow rate, mainly in A zones where the hydrodynamic
 impact is higher. However, similar values on the two days were observed in the group
 injected at a 10 ml/s flow rate. In addition, higher values of apparent iE were also
 observed in the group of 10 ml/s compared to the groups of 20 ml/s, suggesting that
 milder injection conditions must offer cell advantages for gene expression, and
 confirming that outflow obstruction⁷ must contribute to increase the efficiency of
 hydrodynamic liver gene delivery. Interestingly, when the lowest flow was employed
 (1 ml/s), the apparent iE was dramatically reduced up to 5 orders of magnitude,
 suggesting that in these conditions the efficiency of the hydrodynamic procedure is very
 low. This finding supports our previous statement that the amount of gene delivered was

292 in great part not able to be functional. We hypothesize, based on these results that, all
293 the procedures of DNA injection with ≥ 10 ml/s mediate a similar efficacy of
294 transcription, as index of transcription shows, and that the special watertight conditions
295 must probably be contributing to reduce the minimum necessary requirements to reach
296 the hydrodynamic gene transfer. However, the more extreme conditions (more speed
297 and volume) contribute to an increase of DNA copies in the tissue (index of apparent
298 gene delivery) but whose functionality (ability of expressing the gene) must probably be
299 limited, since the apparent intrinsic efficacy is lower regarding the milder conditions
300 group (10ml/s). In any case, the mechanism of anadromous gene transfer mediated by
301 hydrodynamic injection remains unclear.

302 Previously, our group (employing simultaneous portal and cava vein pressures and
303 intravital microscopic evaluation of sinusoidal blood circulation) described that the
304 mechanism of hydrodynamic liver gene transfer involves the inversion of sinusoidal
305 blood flow due to transient inversion of portal versus cava vein differential pressures.
306 Also, morphological changes were associated to the intrahepatic pressures, mainly an
307 increased diameter of the sinusoids and Disse space, as well as increased endothelial
308 disruption and the presence of abundant endocytic vesicles in the apical pole of
309 hepatocytes⁸. The rapid increase in both the inferior cava and portal vein pressures
310 mediated by hydrodynamic injection suggests a low vascular resistance, but pressure in
311 the inferior cava vein remains higher for fewer minutes, resulting in an inverted
312 sinusoidal flow. More recently, it has been proposed¹⁷ that during hydrodynamic
313 injection, retrograde DNA solution reaches the portal vein, where the vascular
314 resistance of the intestinal, splenic and pancreatic capillary beds provides efficient
315 outflow obstruction from the portal vein, and thus outflow obstruction is a necessary
316 condition for effective hydrodynamic gene delivery to individual liver segments or
317 lobes^{7,18}. The results of the present paper confirm in human “ex vivo” liver segments
318 that outflow obstruction in hydrodynamic injection of the eGFP gene results in wide
319 gene delivery and efficient gene expression.

320 The exact mechanism of gene delivery mediated by hydrodynamic injection remains
321 unknown, but two routes of entry of DNA plasmids into hepatocytes have been
322 suggested: plasma membrane rupture¹⁹ and increased membrane permeation^{5,8,20,21},
323 possibly through endocytic vesicles. In the present study we confirm that hydrodynamic
324 injection mediates an increase in sinusoid diameter, with an endothelium that combines
325 both continuous and discontinuous zones, though in no case was generalized disruption

326 observed. In addition, the usually narrow Disse space presented an expanded aspect
327 compatible with an increased flow/pressure in this territory. Although some endocytic
328 vesicles or at least incipient vesicles were observed in the apical membrane of
329 hepatocytes, we failed to find territories with abundant endocytic processes lining the
330 hepatocyte membrane, as previously described in mouse and pig. We do not know the
331 reason for this difference, and although it could be due to species-related structural
332 differences, the “ex vivo” conditions also imply that liver segments were deprived of
333 vascular supply 2-3 hours before hydrodynamic injection, and therefore a loss of cell
334 endocytic response could be possible. However, we cannot exclude that these
335 discrepancies could be due to suboptimal conditions of the experimental model that
336 could be improved. Although the degree of endocytic vesicles could limit the efficiency
337 of the process, this fact could be compensated by an increase of membrane permeation
338 due to the special conditions of the hepatic segments in our experiments.

339 To evaluate how this circumstance could contribute to minimal rupture of the plasma
340 cell membrane of hepatocytes permitting DNA entry into the cell, additional
341 experiments were performed, injecting gold nanoparticles with a mean diameter of 15
342 nm. The results indicate that the nanoparticles were always located in the vascular bed
343 and within the Disse space, but never inside hepatocytes - thus supporting the idea that a
344 permeation process must be involved in the gene transfer process. In this context,
345 facilitated permeation is related to the ability of DNA to cross the cell membrane in the
346 particular scenario of hydrodynamic injection. Two questions must be remarked.

347 Although nanoparticles and plasmid size could be similar, the rigidity characteristics are
348 very different and this could explain their different ability to cross the cell membranes.
349 The second point is that higher concentrations of injected nanoparticles could contribute
350 to clarify the degree of membrane permeation to these particles.

351 In summary, we have shown that the retrograde venous injection of “ex vivo” human
352 liver segments is an anadromous procedure that can mediate good efficacy of gene
353 delivery and gene expression in human liver, with potential clinical applications. In this
354 respect, we believe that this gene transfer procedure could be a promising option in the
355 field of human liver transplantation, since genetically modified grafts could contribute
356 to decrease ischemia-reperfusion injury or prevent allograft rejection, as recently
357 suggested²².

358
359

360 MATERIAL AND METHODS

361 *Liver segments*

362 Human liver segments were obtained from surgical resections of tumor metastatic
363 patients. The liver segments come from surgery to patients and the fragments resected
364 are sealed as well as the remaining piece of liver inside the patient, in the manner the
365 surgeons usually do in the clinical practice: the liver parenchyma was sealed by 3/0 silk
366 sutures or staples when the vessels were bigger than 2-3 mm and by electrocautery
367 when smaller.

368 The number of segments used in the eGFP molecular studies were 19, corresponding to
369 19 human livers. 14 Samples of 10 of those segments were used for fluorescence or
370 immunohistochemistry. Finally, for ultrastructural changes studies without (n=3) or
371 with gold nanoparticles (n=3), 6 additional human liver segments were employed.
372 Table 1 shows the main characteristics of all the human liver segments (HL) employed,
373 including anatomical situation, segment weight, the experimental injection conditions
374 performed and the kind of analyses in each segment, being PCR, molecular analyses of
375 PCR and/or RT-PCR; F, optical fluorescence microscopy for eGFP protein; IHC,
376 optical microscopy for immunohistochemistry of eGFP protein; TEM, transmission
377 electron microscopy; TEM-Gold, transmission electron microscopy after gold
378 nanoparticles injection.

379 We state that the Declaration of Helsinki protocols were followed and that patients gave
380 their written, informed consent. This research was approved by the Clinical Research
381 Ethics Committee of the Hospital Clínico Universitario of Valencia (Spain).

382

383 *Reagents*

384 The primary anti-GFP antibody was obtained from Abcam (ab290, Cambridge, USA),
385 and the peroxidase-conjugated antibody and immunohistochemical developing system
386 (LSAB) were obtained from DAKO (Barcelona, Spain).

387 The plasmid p3C-EGFP (6.45 Kb), containing the enhanced green fluorescent protein
388 cDNA driven by the pCMV promoter, was constructed by cloning EGFP into the
389 HindIII site of pcDNA3 (Invitrogen, Barcelona, Spain), excised from pEGFP-N1 (4.7
390 kb) plasmid vector (Clontech Laboratories, Saint-Germain-en-Laye, France).

391

392 *Gold nanoparticle synthesis*

393 All chemicals were purchased from Sigma-Aldrich (Madrid, Spain) and used as
394 received without further purification. Gold nanoparticles were synthesized following a
395 modification of the Turkevich method²³. Typically, 0.4 g of HAuCl₄·3H₂O were
396 dissolved in 90 ml of water in a two-neck round flask (1.3 mM HAuCl₄). The resulting
397 solution was heated to boiling and refluxed. Then, 9 ml of a 47.2 mM sodium citrate
398 solution (0.125 g sodium citrate in 9 ml water) was preheated and quickly added. The
399 solution turned from yellow to black and to deep red. After the color changed, the
400 solution was refluxed for 20 minutes. Then, the heater was turned off and the solution
401 was stirred until it reached room temperature. The resulting solution was diluted with
402 water to a final volume of 500 ml. Gold nanoparticles were characterized by
403 transmission electron microscopy (TEM, Jeol 1010, Tokyo, Japan). The average
404 diameter and the size distribution of the gold nanoparticles were determined from TEM
405 images by counting at least 300 nanoparticles using Image Pro Plus software from
406 Media Cybernetics (Bethesda, USA).

407

408 *“Ex vivo” gene transfer to liver segment*

409 Human liver segments (418.0±227.2 g) were obtained from patients after surgical
410 resection of liver metastases. Samples were immediately transported under humid and
411 sterile box conditions to the laboratory, and all experimental processing was completed
412 in approximately 1.5 hours, employing sterile solutions and aseptic conditions. A
413 flexible 8F introducer (used as catheter), filled with saline solution, was placed into the
414 hepatic vein previously marked by the surgeon. After catheter fixation using needle and
415 thread, in all experiments, contrast solution was injected before hydrodynamic injection
416 to confirm a correct positioning of the catheter and balloon closure of the vein. Always,
417 the contrast injection was at low speed (not hydrodynamical) and employing a
418 maximum volume of approximately 1% of segment weight (3-10ml). The visualization
419 of a well defined vascular tree was required before performing the hydrodynamic
420 injection.

421 For gene transfer study, a volume of 1/5 or 1/10 of the segment weight, bearing 20
422 µg/ml of plasmid in saline solution containing the green fluorescent protein gene
423 (eGFP) was injected at a 10 or 20 ml/s flow rate. A low injection flow group was also
424 included being injected at 1 ml/s and with the highest volume, 1/5. During the
425 experiment of hydrodynamic injection, the pressure (mm Hg) at the tip of the introducer
426 was continuously monitorized by means of an auxiliary access. A Spectramed Statham

pressure transducer (model P23XL) and a Grass model 7 polygraph (preamplifier model 7P1J and amplifier model 7DAG) were employed. After injection, we wait five minutes to remove the catheter.

Then, tissue samples were obtained from perfused areas. Tissue samples < 1 mm in thickness were subsequently collected under sterile conditions and cultured in DMEM medium and a 5% CO₂ atmosphere. Samples were removed 1 and 2 days after transfection and processed for molecular analysis to evaluate the efficiency of gene delivery and the persistence of eGFP expression.

For morphological studies, the same procedure was performed, but injecting a solution containing 15 nm gold nanoparticles (1.8x10¹² Au particles/ml) for further electron microscopy observations.

Quantitative PCR and RT-PCR

Liver tissue samples were cut into small pieces and homogenized in Tri Reagent (Ambion, Applied Biosystems, Madrid, Spain) with an Ultra-Turrax (Hielscher Ultrasonics GmbH, Teltow, Germany) homogenizer. Subsequently, the RNA samples were treated with RNase free DNase (Gibco, Invitrogen, Barcelona, Spain). Further purification with the RNeasy mini-kit (Qiagen, Barcelona, Spain) was performed before spectrophotometric quantification. Retrotranscription to cDNA was performed using 1 µg total RNA (DNA free), Random Hexamers and a High Capacity cDNA Archive kit (Applied Biosystems, Madrid, Spain). For qRT-PCR, power SYBR green PCR master mix (Applied Biosystems, Madrid, Spain) was employed according to the instructions of the manufacturer.

The oligonucleotides were designed with Primer Express software (Applied Biosystems, Madrid, Spain). The primers specific for eGFP were:

FW: 5'-GTA AAC GGC CAC AAG TTC AGC-3', Tm: 53.9 °C

RV: 5'-TGG TGC AGA TGA ACT TCA GGG-3', Tm: 54.9 °C

Probe: 5'-6FAM-CTTGCCGTAGGTGGC-MGBNFQ-3'

The precise amount of RNA (based on optical density) and its quality (lack of degradation) were normalized with respect to an endogenous control gene (GAPDH).

The quantitative data were calculated as the number of DNA or RNA copies on a regression curve employing the plasmid containing the eGFP gene or full human DNA, considering that 3 pg of DNA contains a genome copy¹⁶.

461 Statistically significant differences between groups were evaluated by two-way analysis
462 of variance (ANOVA) followed by Bonferroni post-tests, employing Graph Pad Prism
463 4.02 Software (GraphPad Software, San Diego, California, USA).

464

465 *Fluorescent and immunohistochemical eGFP identification*

466 For fluorescent study, liver cryosections from human segments (n=7) cultured 24 h after
467 transfection were used. The cryosections were examined and photographed using a
468 Zeiss Axiovert 135 inverted microscope (Carl Zeiss, Madrid, Spain).

469 For immunohistochemical study, liver samples (n=7) were fixed in 4%
470 paraformaldehyde and embedded in paraffin. Immunostaining was carried out as
471 previously described². Briefly, deparaffinized tissue sections were incubated with 4%
472 bovine serum albumin in PBS (1 hour, 37°C). Then, the tissue sections were incubated
473 in antibody solution (1:300 diluted rabbit anti-GFP) at 37°C for one hour. The
474 respective control samples incubated in the absence of specific antibody were included.
475 Detection was carried out using the LSAB-2 peroxidase kit (Dako, Barcelona, Spain).
476 Tissue was counterstained with hematoxylin before dehydration.

477

478 *Electron microscopy*

479 Human liver segments (n=3) were retrodynamically injected (volume 1/5 of segment
480 weight) through the catheter placed in the hepatic vein with a buffered solution of 2.5%
481 glutaraldehyde. Additional experiments (n=3) were performed under identical
482 conditions of glutaraldehyde injection but containing 10¹² gold particles/ml, to study the
483 liver distribution of 15 nm gold nanoparticles after injection. Then, in both cases small
484 tissue pieces from different liver areas were removed and immersed in phosphate
485 Sørensen buffer (pH 7.4) solution containing 2.5% glutaraldehyde. For transmission
486 electron microscopy, multiple 1-mm³ pieces of liver were routinely processed and
487 embedded in Epoxy resin. Ultrathin sections, stained with uranyl acetate and lead
488 citrate, were examined under a Jeol JEM-1010 electron microscope.

489

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499 REFERENCES

- 500 1. Liu F, Song YK, Liu D. Hydrodynamics-based transfection in animals by systemic
501 administration of plasmid DNA. *Gene Ther* 1999; **6**: 1258-1266
- 502 2. Aliño SF, Crespo A, Dasí F. Long-term therapeutic levels of human alpha-1-
503 antitrypsin in plasma after hydrodynamic injection of nonviral DNA. *Gene Ther* 2003;
504 **10**: 1672-1679
- 505 3. Khorsandi SE, Bachellier P, Weber JC, Greget M, Jaeck D, Zacharoulis D, *et al.*
506 Minimally invasive and selective hydrodynamic gene therapy of liver segments in the
507 pig and human. *Cancer Gene Ther* 2008; **15**: 225-30.
- 508 4. Herrero MJ, Dasi F, Noguera I, Sanchez M., Moret I., Sanmartin I, *et al.* Mouse and
509 pig nonviral liver gene therapy: success and trials. *Gene Ther Mol Biol* 2005; **9**: 169–
510 180.
- 511 5. Aliño SF, Herrero MJ, Noguera I, Dasi F, Sanchez M. Pig liver gene therapy by
512 noninvasive interventionis cathetherism. *Gene Ther* 2007; **14**: 334-343
- 513 6. Aliño SF, Herrero MJ, Bodi V, Noguera I, Mainar L, Dasi F, *et al.* Naked DNA
514 delivery to whole pig cardiac tissue by coronary sinus retrograde injection employing
515 non-invasive catheterization. *J Gene Med* 2010; **12**: 920-926
- 516 7. Sawyer GJ, Zhang X, Fabre JW. Technical requirements for effective regional
517 hydrodynamic gene delivery to the left lateral lobe of the rat liver. *Gene Ther* 2010; **17**:
518 560-564
- 519 8. Crespo A, Peydro A, Dasi F, Benet M, Calvete JJ, Revert F, *et al.* Hydrodynamic
520 liver gene transfer mechanism involves transient sinusoidal blood stasis and massive
521 endocytic vesicles, *Gene Ther* 2005; **12**: 927-935
- 522 9. McTiernan CF, Mathier MA, Zhu X, Xiao X, Klein E, Swan CH, *et al.* Myocarditis
523 following adeno-associated viral gene expression of human soluble TNF receptor
524 (TNFR_{II}-Fc) in baboon hearts, *GeneTher* 2007; **14**: 1613–1622
- 525 10. Zhang G, Budker V, Wolf JA. High levels of foreign gene expression in hepatocytes
526 after tail vein injections of naked plasmid DNA. *Hum Gene Ther* 1999; **10**: 1735-1737
- 527 11. Hoshino K, Kimura T, De Grand AM, Yoneyama R, Kawase Y, Houser S, *et al.*
528 Three catheter-based strategies for cardiac delivery of therapeutic gelatin microspheres.
529 *Gene Therapy* 2006; **13**: 1320-1327
- 530 12. Suda T, Suda K, Liu D. Computer-assisted hydrodynamic gene delivery. *Mol Ther*
531 2008; **16**: 1098-1104

532 13. Fabre JW, Grehan A, Whiterhorne M, Sawyer GJ, Dong X, Salehi S, *et al.*
533 Hydrodynamic gene delivery to the pig liver via an isolated segment of the inferior vena
534 cava. *Gene Ther* 2008; **15**: 452-462

535 14. Kamimura K, Suda T, Xu W, Zhang G, Liu D. Image-guide, lobe-sapecific
536 hydrodynamic gene delivery to swine liver. *Mol Ther* 2009; **17**: 491-499

537 15. Eastman SJ, Baskin KM, Hodges BL, Chu Q, Gates A, Dreusicke R, *et al.*
538 Development of catheter-based procedures for transducing the isolated rabbit liver with
539 plasmid DNA. *Hum Gene Ther* 2002; **13**: 2065-2077.

540 16. Gregory, TR. Animal Genome Size Database (2010). <http://www.genomesize.com>
541 (accessed on April 2010)

542 17. Sawyer GJ, Rela M, Davenport M, Whitehorne M, Zhang X, Fabre JW.
543 Hydrodynamic gene delivery to the liver: theoretical and practical issues for clinical
544 application. *Curr Gene Ther* 2009; **9**: 128-135.

545 18. Fabre JW, Whitehorne M, Grehan A, Sawyer GF, Zhang X, Davenport M, *et al.*
546 Critical physiological and surgical considerations for hydrodynamic pressurisation of
547 individual segments of the pig liver. *Human Gene Ther* 2010; e-pub ahead of print
548 doi:10.1089/hum.2010.144

549 19. Zhang G, Gao X, Song YK, Volimer R, Stolz DB, Gasiorowski JZ, *et al.*
550 Hydroporation as the mechanism of hydrodynamic delivery. *Gene Ther* 2004; **11**: 675-
551 682.

552 20. Sebestyén MG, Budker VG, Budker T, Subbotin VM, Zhang G, Monahan SD, *et al.*
553 Mechanism of plasmid delivery by hydrodynamic tail vein injection. I.Hepatocyte
554 uptake of various molecules. *J Gene Med* 2006; **8**: 852-873

555 21. Suda T, Gao X, Stolz DB, Liu D. Structural impact of hydrodynamic injection on
556 mouse liver. *Gene Ther* 2007; **14**: 129-137.

557 22. Si ZZ, Li JQ, Ai HA, He ZJ, Hu W, Li YN. Recombinant adenovirus vector Ad-
558 hIL-10 protects grafts from cold ischemia-reperfusion injury following orthotopic liver
559 transplantation in rats. *Heptobiliar Pacreatic Dis Int* 2010; **9**: 144.148

560 23. Kimling J, Maier M, Okenve B, Kotaidis V, Ballot H, Plech A. Turkevich method for
561 gold nanoparticle synthesis revisited. *J Phys Chem* 2006; **110**: 157-60

562

563

564 FIGURE LEGENDS

565

566 **Figure 1- Catheter position in liver segment**

567 Representative image of Rx fluoroscopy of the catheter placed inside hepatic vein of a
568 liver segment (A) corresponding to VII and VIII human hepatic liver segments,
569 weighting 450g, as compared with the anatomical image of the same liver segment (B),
570 where the cuts represent the places where samples were removed for morphological and
571 molecular analysis, after hydrodynamic injection, being A zone the cut in the middle of
572 the segment corresponding to direct site of injection, and B zone those upper and lower
573 cut corresponding to lateral zones. The small black bars in A panel are the staples used
574 by the surgeon to close the vessels when surgery was performed. C and D panels show
575 the Rx image at the same segment during injection of contrast solution at low speed
576 ($<1\text{ ml/s}$, not hydrodynamical) with total volume of 5ml. C panel shows the picture taken
577 with half of the volume injected and D panel, the picture taken at the end of injection.

578

579 **Figure 2- Fluorescence and immunohistochemistry of eGFP**

580 The fluorescence and immunohistochemistry findings of eGFP in histological liver
581 sections are shown. In the first case (Fig. 2A-C), a saline solution containing the
582 plasmid DNA was injected to liver segment at a 20 ml/s flow rate, with a final volume
583 of 1/10 segment weight. The liver samples were cultured 24 h, then frozen, and the
584 cryosections were used for fluorescent microscopy. The figure shows representative
585 images under x20 magnification. In the second case (Fig. 2E-G), the liver segment was
586 injected at a 10 ml/s flow rate, with a final volume of 1/5 segment weight. After 24 h of
587 culture, eGFP protein was developed by immunohistochemistry in paraffin sections
588 from formalin-fixed tissue. E: image from control immunohistochemical tissue section,
589 developed in the absence of specific primary antibody. F and G: specific
590 immunohistochemical reaction against eGFP protein under x40 magnification.
591 Detection was carried out using the LSAB-2 peroxidase kit. Tissue was counterstained
592 with hematoxylin. Images D and H show the respective experiments of fluorescence and
593 immunohistochemistry from liver segments injected at 1 ml/s flow rate and with 1/5
594 segment weight volume.

595

596

597

Figure 3- Index of Apparent Gene Delivery and Index of Tissue Transcription

The human liver segments were retrogradely injected with saline solution containing 20 µg/ml of DNA plasmid bearing the eGFP gene. Different groups were established according to the different conditions of flow rate (1, 10 or 20 ml/s) and total volume injected (1/5 or 1/10 of segment weight, g). Quantitative eGFP PCR or RT-PCR was performed in liver tissue samples collected 1 and 2 days after gene transfer from zones A and B, and the eGFP copy number in each sample was calculated on a standard curve using the same transfection plasmid. The index of apparent eGFP gene delivery to liver tissue (Fig. 3A) was calculated as the ratio of eGFP DNA copies per 100 pg of total DNA. Statistical significance by two-way ANOVA analysis and Bonferroni post-test was found in groups marked with * ($p < 0,01$) compared to 20 ml/s, 1/5 group. The index of tissue transcription (Fig. 3B) was calculated as the number of eGFP RNA copies per 100 pg of total RNA. No statistically significant differences were observed between groups except for 1 ml/s, 1/5 ($p < 0,05$) by two-way ANOVA and Bonferroni post-test, marked with *.

Figure 4- Index of Apparent Gene Intrinsic Efficacy in Liver Tissue

Experimental conditions of transfection and molecular analysis of the liver samples were as described in Figure 3. The index of apparent intrinsic gene efficacy (iE) was calculated as the ratio of RNA/DNA copy of eGFP in each sample, and indicates the amount of RNA produced per DNA gene copy. The statistical significance between groups is indicated as * ($p < 0,01$) when comparing groups against 10 ml/s, 1/5. The symbol # ($p < 0,01$) indicates statistical significance between A and B zones inside the group by two-way ANOVA and Bonferroni post-test.

Figure 5- Ultrastructural morphological changes

The liver segment was retrogradely injected at a 20 ml/s flow rate with a buffered 2.5% glutaraldehyde solution, and tissue samples were taken for transmission electron microscopy. In the middle, a vessel surrounded by hepatocytes is shown at low magnification (bar = 10 µm), and squares indicate the respective areas at higher magnification for identifying morphological changes in vascular endothelium, Disse space and apical hepatocyte membrane. Arrows: discontinuous endothelium; Star: endocytic vesicles or incipient vesicles; White arrow: Disse space; Bar of square b: 500 nm; Bars of squares a, c and d: 1000 nm).

632

633 **Figure 6- Gold nanoparticle characterization**

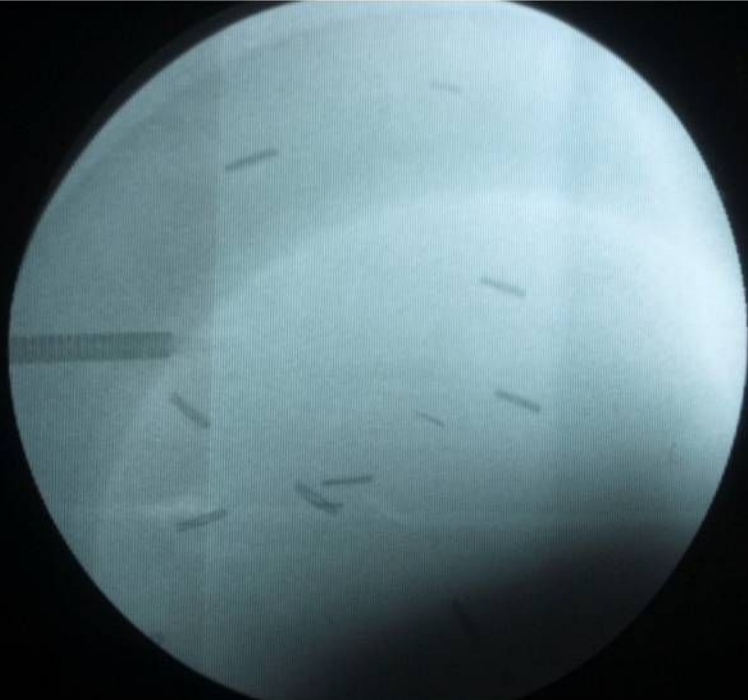
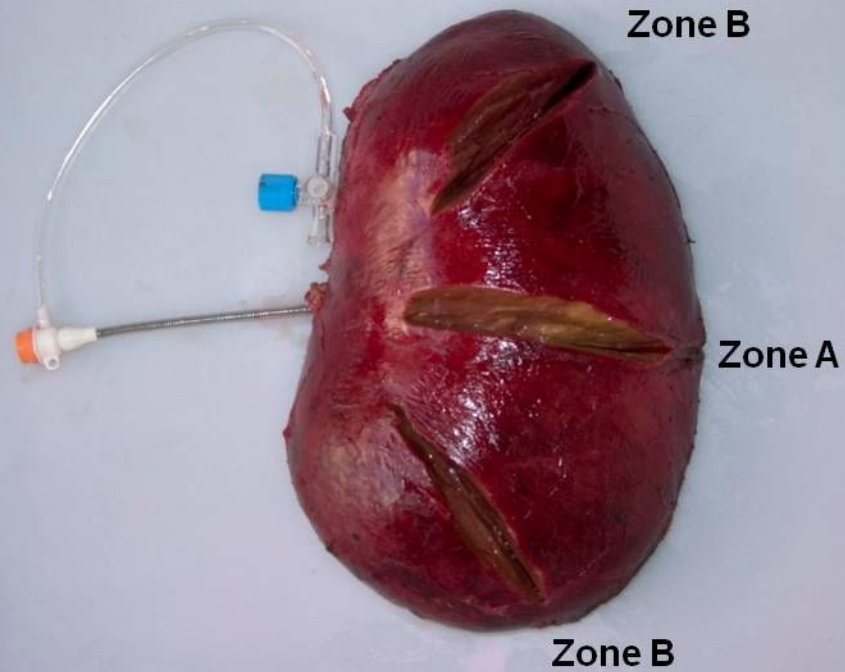
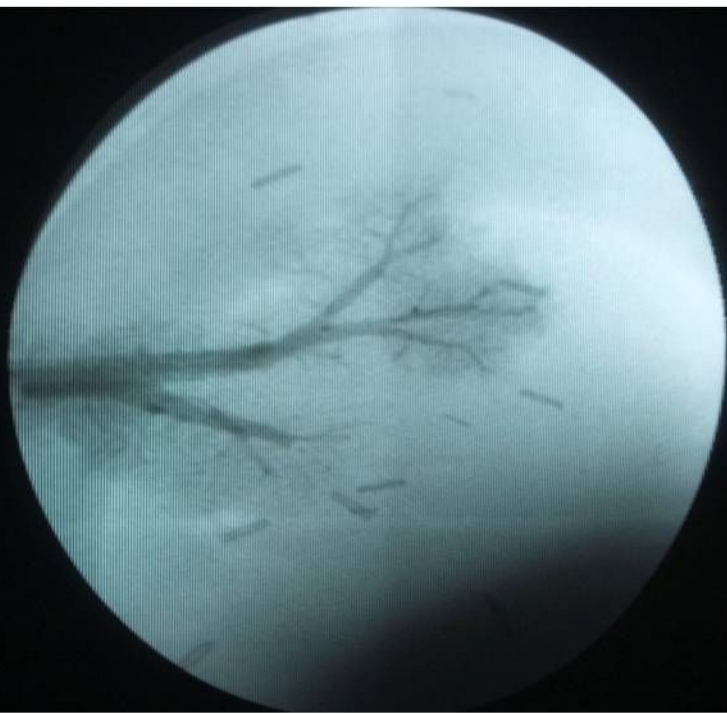
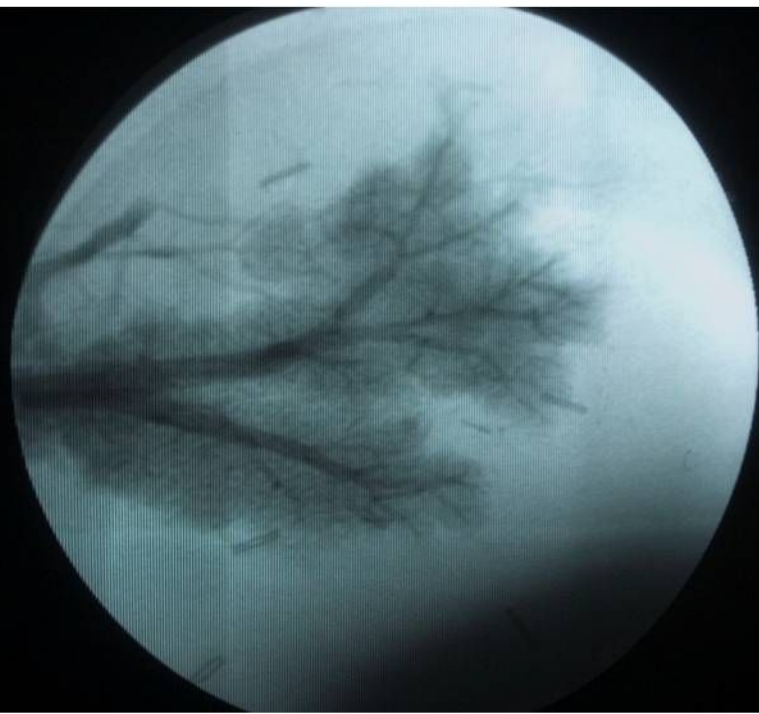
634 The gold nanoparticles were prepared as described in Methods. The morphological
635 characteristics of the gold nanoparticles were examined by transmission electron
636 microscopy (6B), and the average diameter and size distribution (6A) were determined
637 by counting at least 300 nanoparticles.

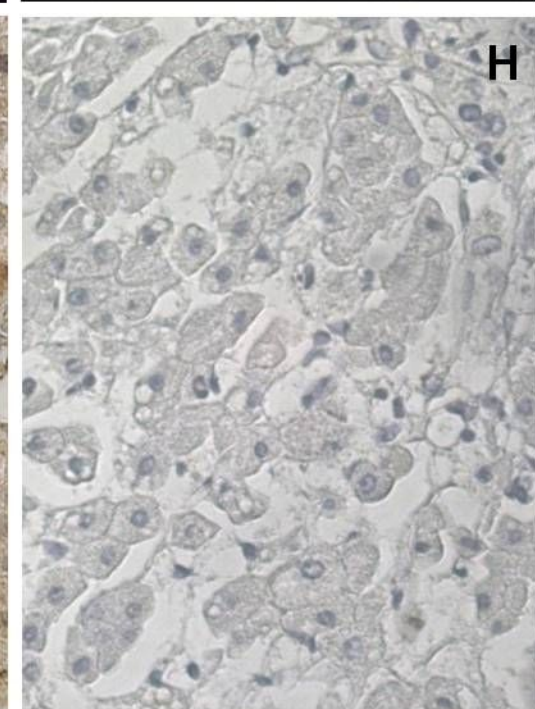
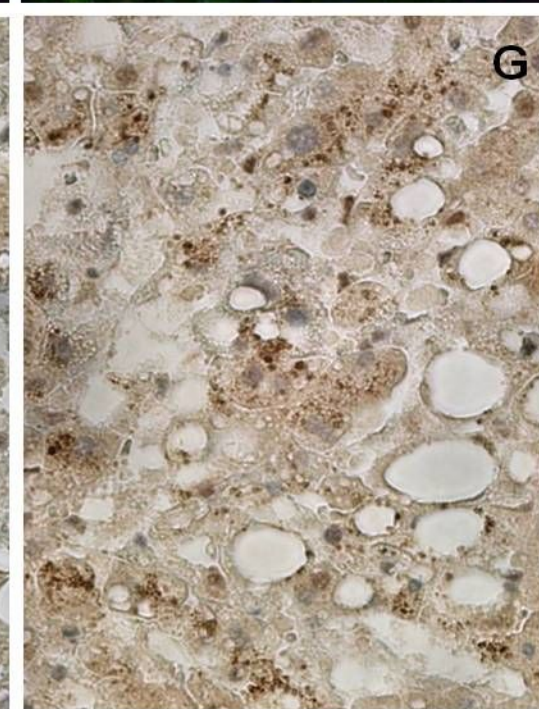
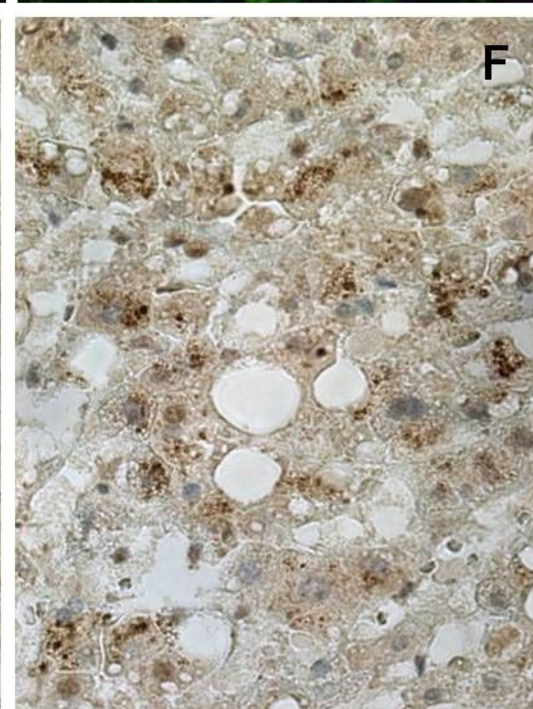
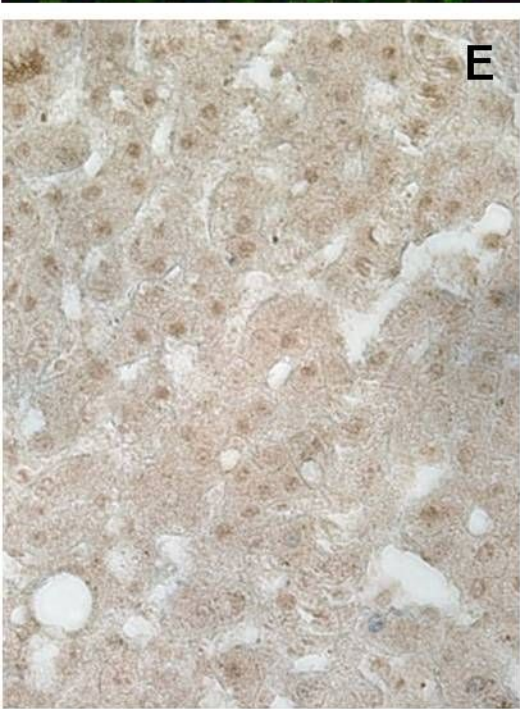
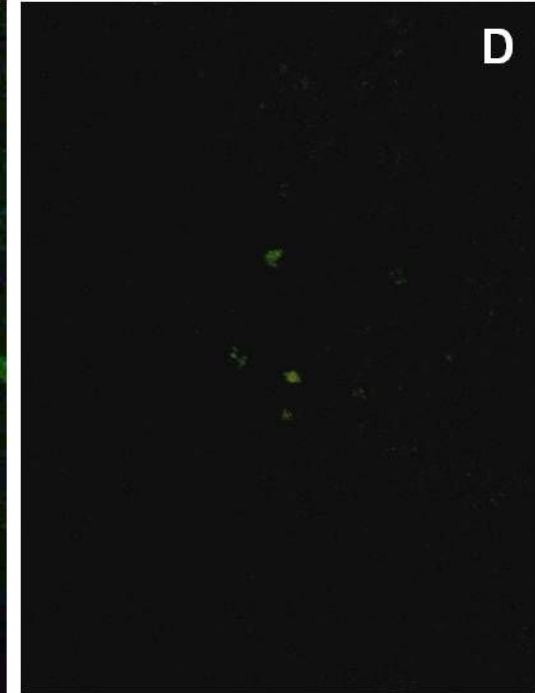
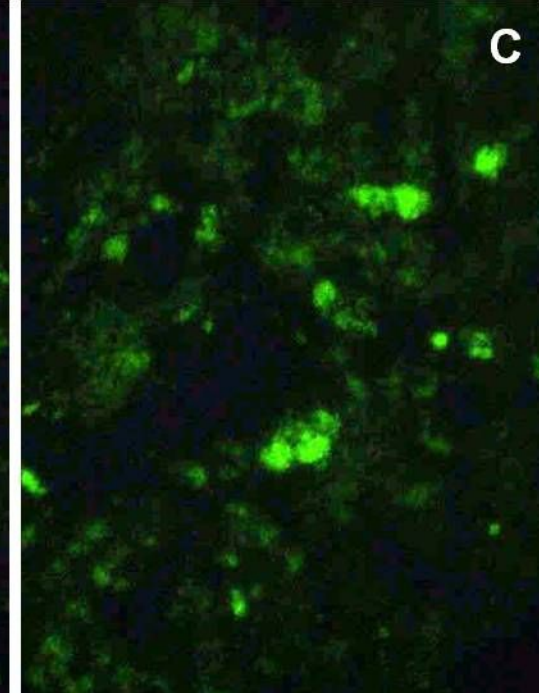
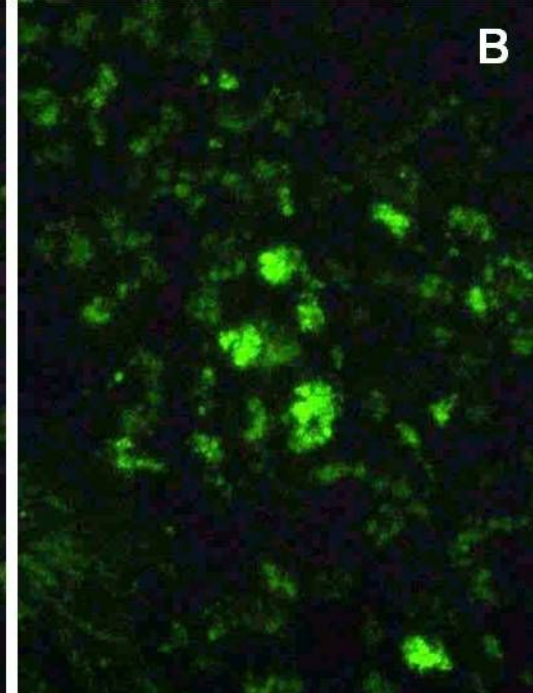
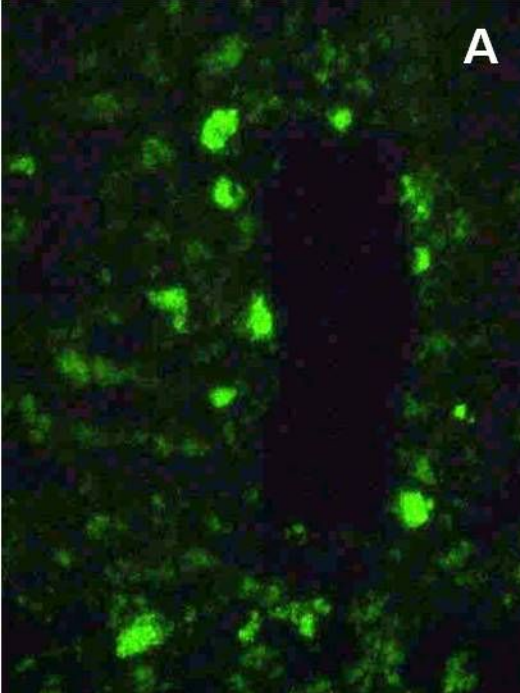
638

639 **Figure 7- Gold nanoparticle distribution in the liver segment**

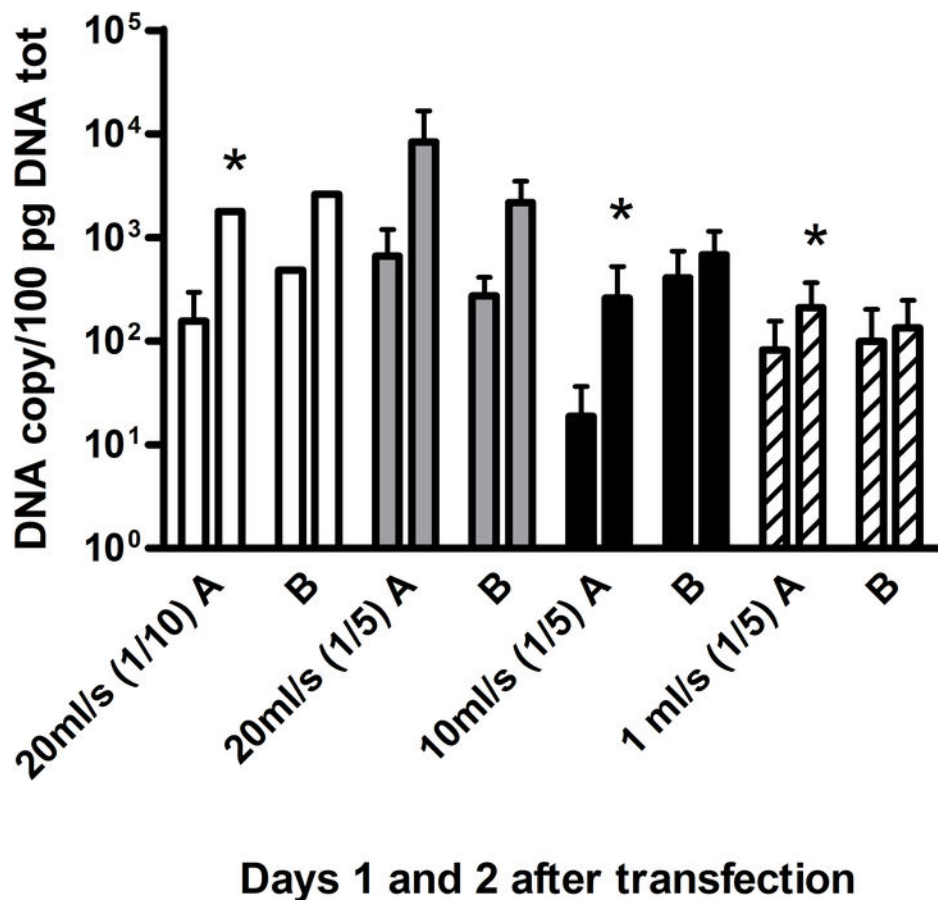
640 The liver segment was retrogradely injected at a 20 ml/s flow rate with buffered 2.5%
641 glutaraldehyde solution plus gold nanoparticles (15 nm in diameter and 10^{12}
642 particles/ml). The central image (at low magnification) shows a dilated sinusoid where
643 specific boxes corresponding to sites of the endothelium-Disse space-hepatocyte (a, b, c,
644 d) are amplified and then again enlarged (a1-a3, b1, c1-c2 and d1) with the aim of
645 identifying the location of nanoparticles. The latter are observed within the sinusoids
646 and the Disse space, but not inside the hepatocytes.

647

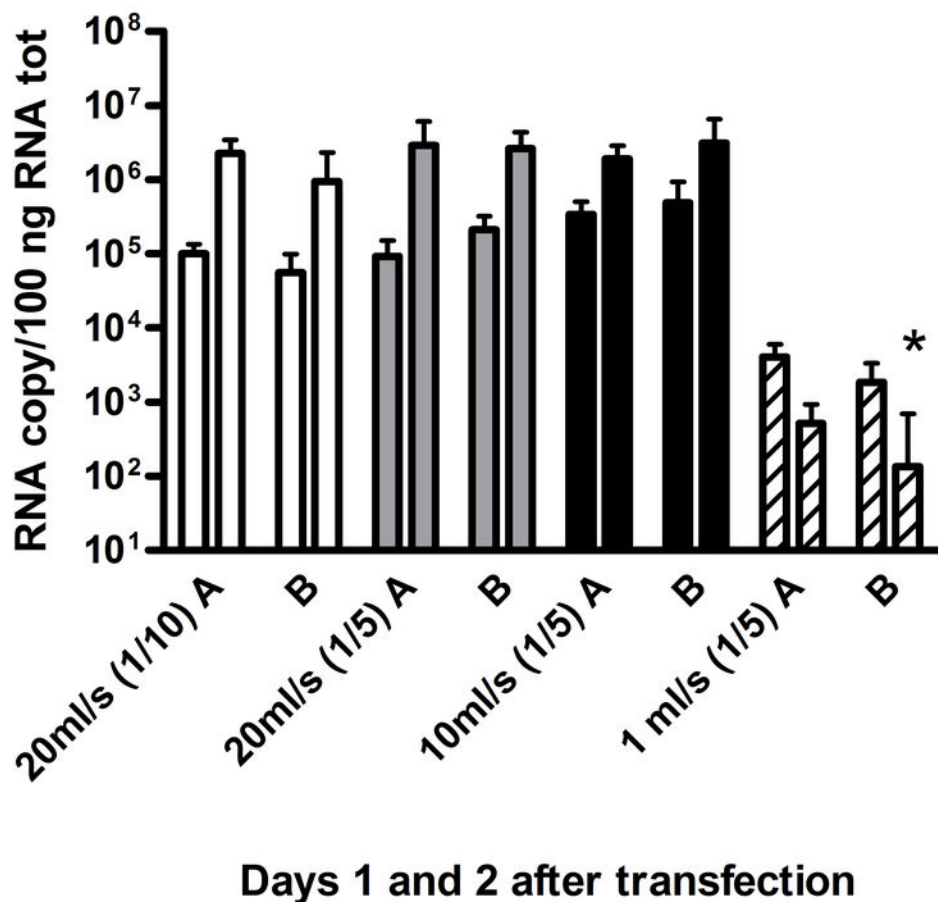
A**B****C****D**



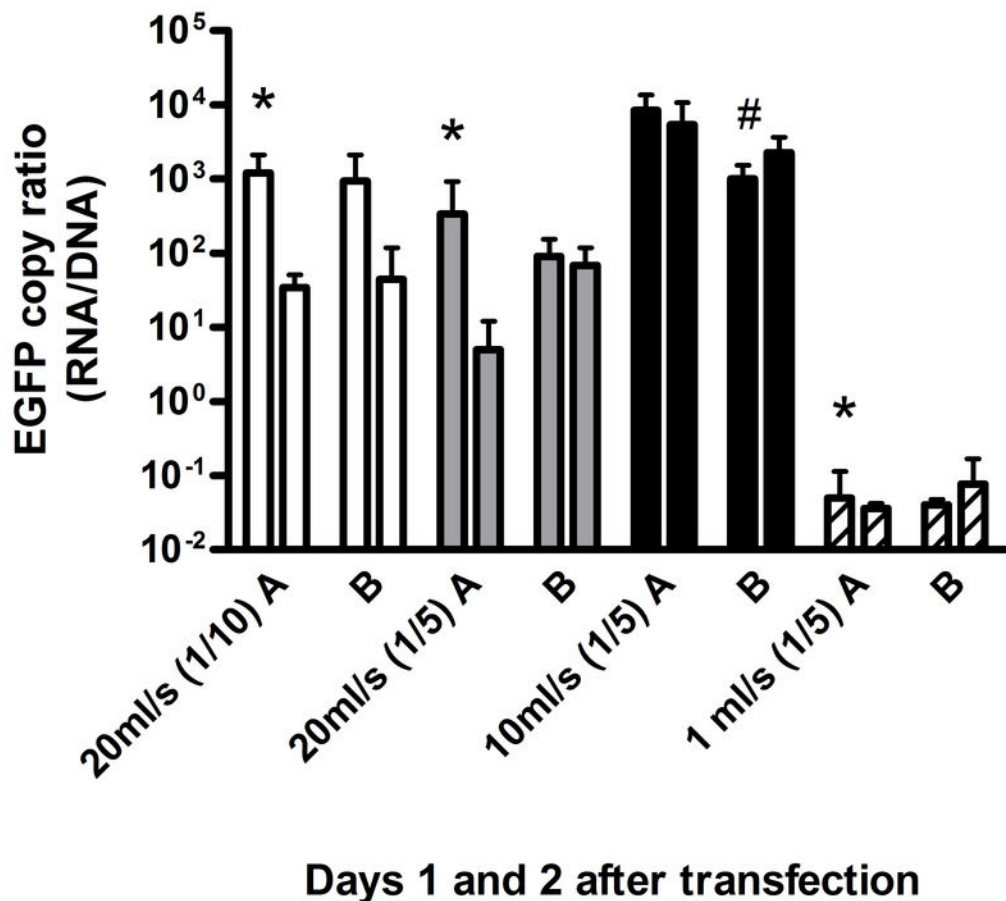
Index of Apparent Gene Delivery

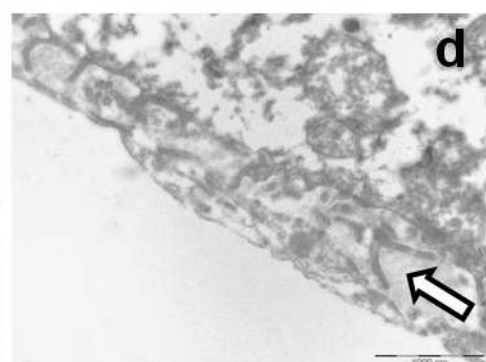
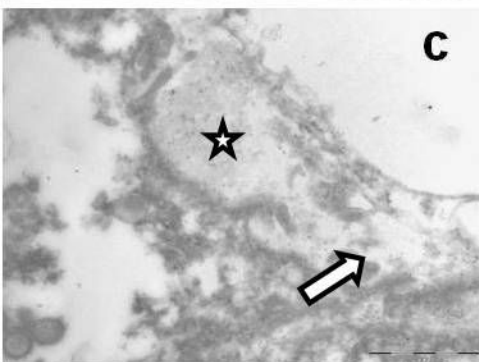
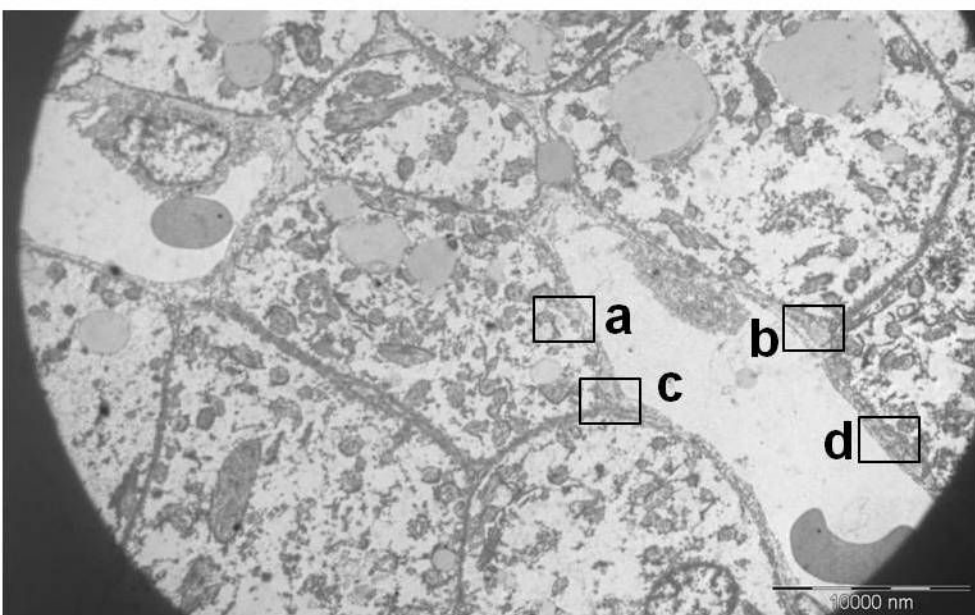
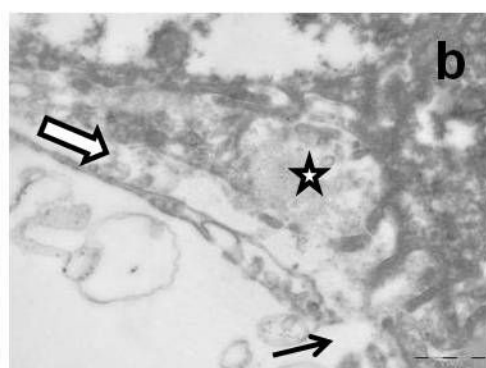
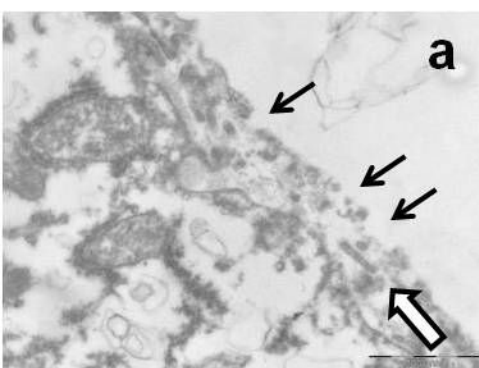


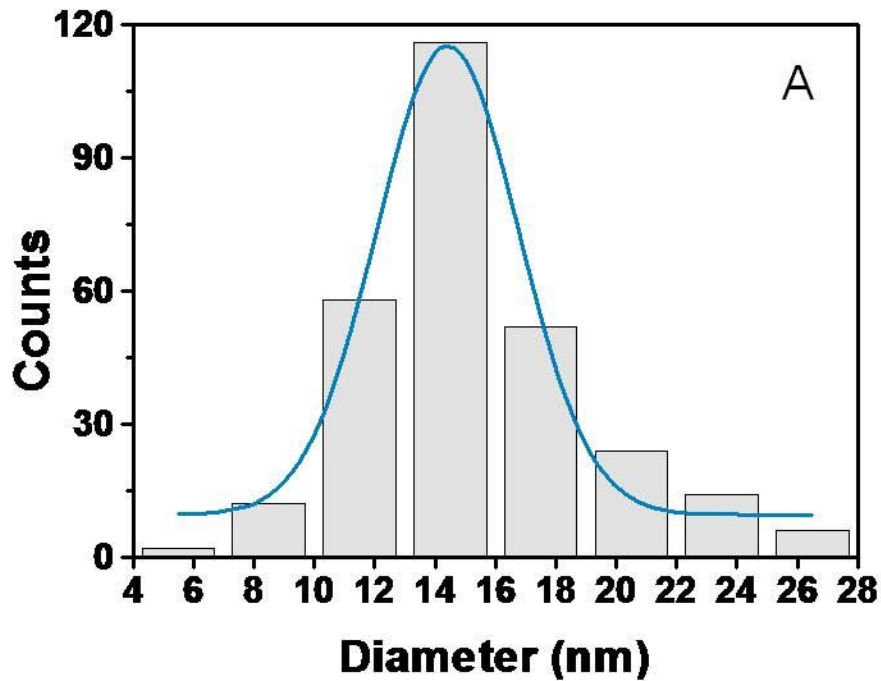
Index of Tissue Transcription

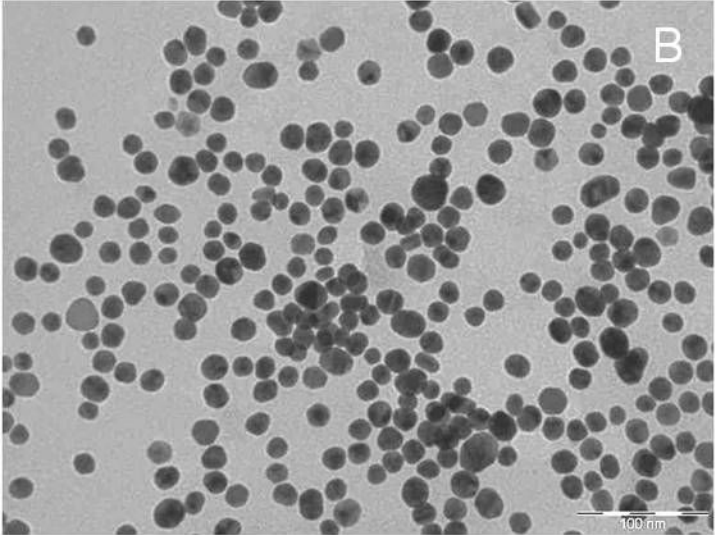


Index of Apparent Gene Intrinsic Efficacy









Au particles - TEM

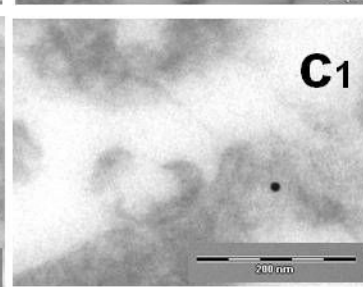
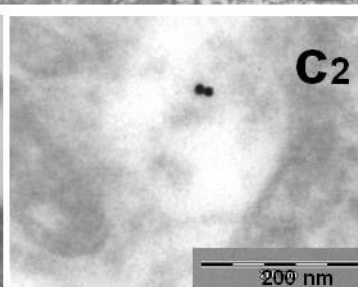
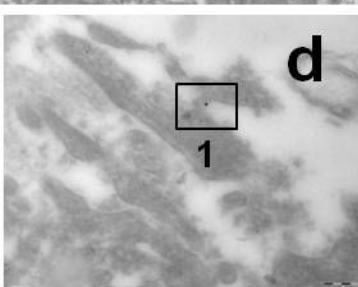
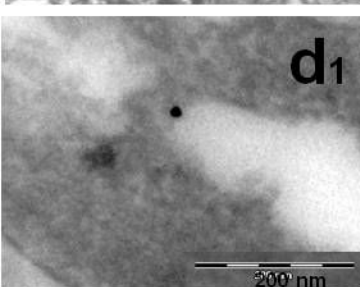
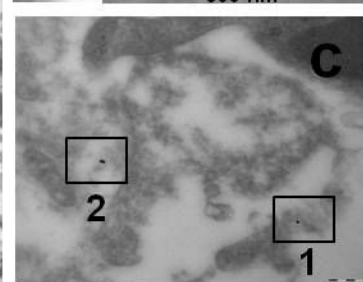
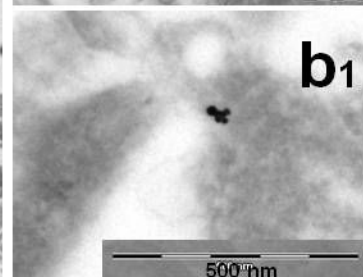
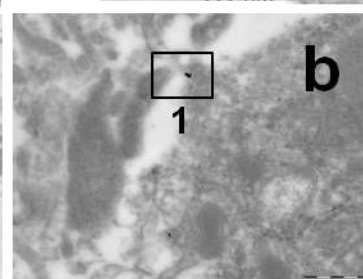
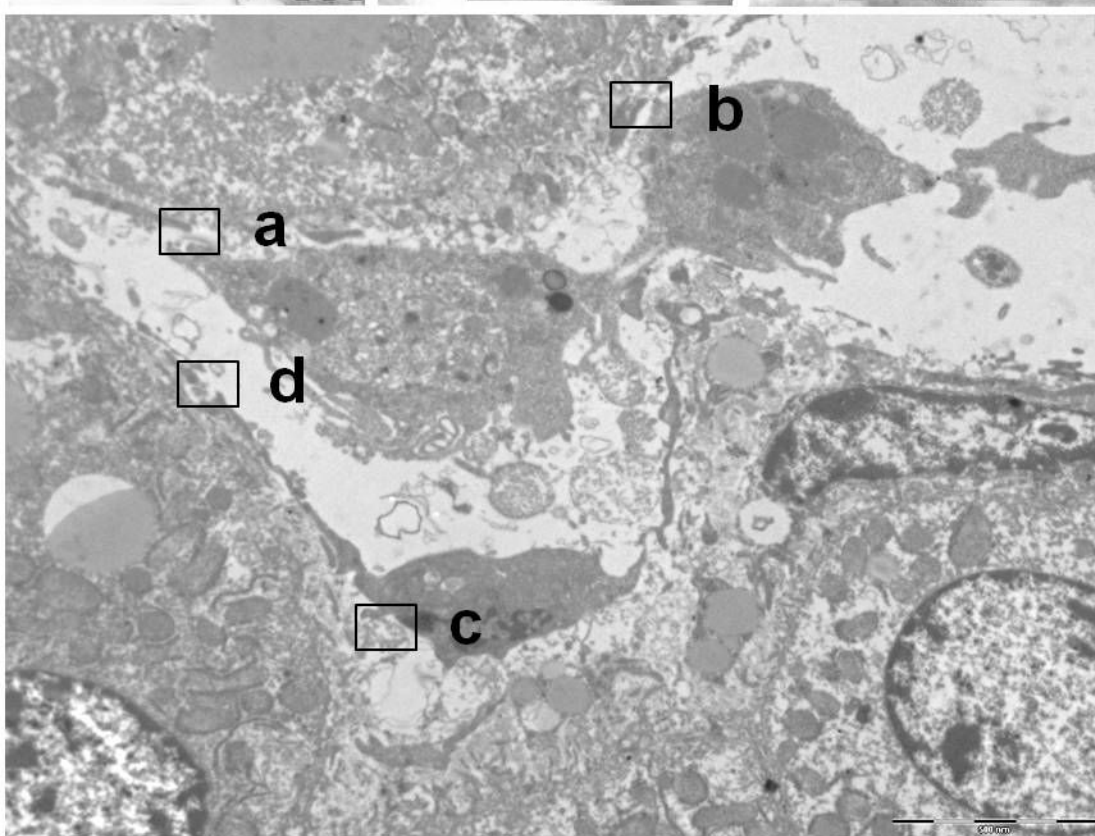
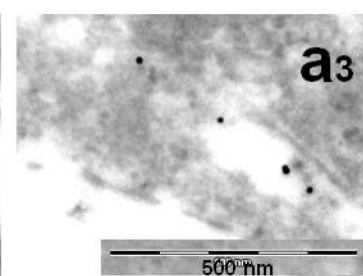
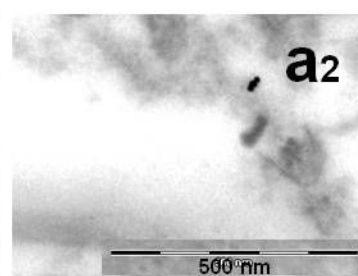
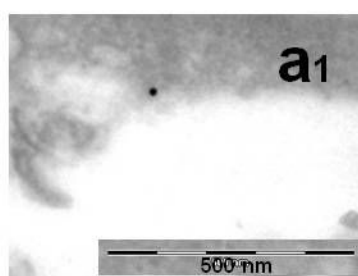
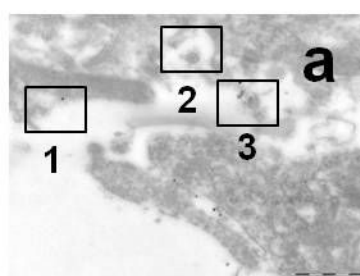


Table 1- Main characteristics of the human liver segments (HL) employed. The table includes the experimental injection conditions performed and the kind of analyses in each segment, being PCR, molecular analyses of PCR and/or RT-PCR; F, optical fluorescence microscopy for eGFP protein; IHC, optical microscopy for immunohistochemistry of eGFP protein; TEM, transmission electron microscopy; TEM-Gold, transmission electron microscopy after gold nanoparticles injection.

Experimental Conditions	Experiment Number	Segment Localization	Segment Weight	Analyses Performed
20ml/s, 1/10 n=5	HL01	VI and VII	500 g	PCR, F
	HL02	VI	404 g	PCR, F
	HL03	VII and VIII	450 g	PCR, F
	HL04	VIII	600 g	PCR
	HL05	II and III	446 g	PCR
20ml/s, 1/5 n=10	HL06	II and III	350 g	PCR
	HL07	II and III	157 g	PCR
	HL08	II and III	302 g	PCR
	HL09	V-VIII	815 g	PCR
	HL10	VII	200 g	TEM
	HL11	VI	310 g	TEM
	HL12	II and III	244 g	TEM
	HL13	VI	294 g	TEM-Gold
	HL14	II and III	440 g	TEM-Gold
	HL15	II and III	290 g	TEM-Gold
10ml/s, 1/5 n=6	HL16	V-VIII	425 g	PCR
	HL17	VIII	110 g	PCR, IHC

	HL18	VI and VII	816 g	PCR,IHC
	HL19	II and III	312 g	PCR,IHC
	HL20	VI and VII	829 g	PCR
	HL21	V-VIII	987 g	PCR
1ml/s, 1/5 (“Control”) n=4	HL22	V	340 g	PCR, F, IHC
	HL23	VI and VII	342 g	PCR, F, IHC
	HL24	II and III	211 g	PCR, F, IHC
	HL25	II and III	277 g	PCR, F, IHC